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㉓ Implant material composition, preparation thereof as well as uses thereof and implant product obtainable therefrom.

㉔ The invention relates to an implant material composition for restoring bone tissue in a human or animal body. Said composition comprises a particulate biocompatible bone tissue substitute material distributed in a bioacceptable mixture of a) a water-based liquid and b) a monoglyceride and optionally c) a triglyceride, said ingredients a), b) and c) forming an L2-phase or a lamellar liquid crystalline phase and being present in such proportions within said phases that they are capable of being transformed into a cubic liquid crystalline phase or a reversed hexagonal liquid crystalline phase when contacted with an aqueous liquid. Thus, the phase conversion referred to imparts to the composition such a high viscosity that it works as an implant material as defined.

There is also provided a method of preparing said composition comprising forming the L2 or lamellar phase and distributing the bone tissue substitute material therein.

Moreover, there is provided a method of restoring lost bone tissue comprising applying the composition to a bone cavity and converting the same by contact with an aqueous liquid.

The composition for use as an implant material composition as well as the use thereof for the manufacture of an implant product are also provided.

Finally the invention relates to the restored implant bone tissue product obtainable from said com-

position by contact with said aqueous liquid.

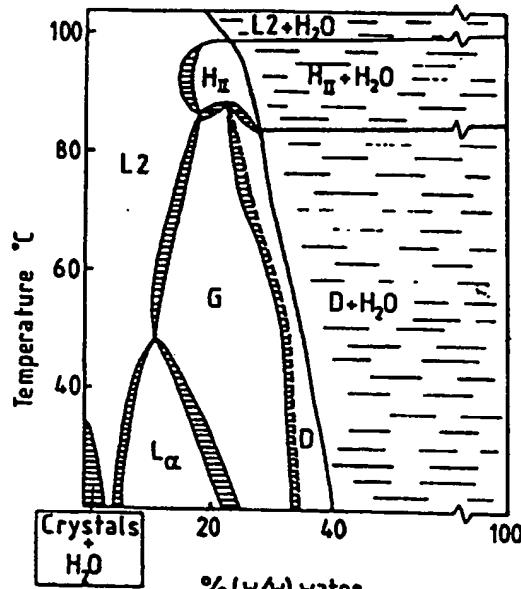


Fig. 1

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**IMPLANT MATERIAL COMPOSITION, PREPARATION THEREOF AS WELL AS USES THEREOF AND
IMPLANT PRODUCT OBTAINABLE THEREFROM:**

Technical field

The present invention relates to the field of implant materials for restoring bone tissues in humans or animals. More specifically the invention relates to a new, easily and consistently applicable implant material composition, to a method of preparing said composition, to uses of the same as well as to an implant product obtainable from said composition.

Background of the invention

The implantation of materials of different types in the human or animal body in order to replace bone portions which have been worn out or which have deteriorated due to diseases of other reasons is steadily increasing. In order to eliminate the risk of having immunological diseases different synthetic materials have come into use within this technical field. As examples of suitable materials used for said purpose there can be mentioned a metal like titanium and minerals and ceramics such as high-purity alumina, tricalcium phosphate and calcium aluminate. In the absence of risks of immunological diseases fragments from natural bone may also be considered in this respect. Especially preferred materials are, however, materials having a chemical composition and crystal structure similar to those of the materials that are built up by the living organism, such as calcium hydroxyapatite. One synthetic material of this type which has come into use for restoring bone tissue is the polycrystalline mineral calcium hydroxyapatite and particularly the non-resorbable type thereof which has the formula $\text{Ca}_{10}(\text{PO}_4)_6(\text{OH})_2$ and which is also one of the main constituents of the bones in the body wherein the organic matrix of the bone tissue is received. Said material serves as a "climb structure" for bone tissue and prevents connective tissues from growing into the region of the bone which has been destroyed and is to be restored.

Calcium hydroxyapatite of the above-mentioned formula is manufactured by Asahi Optical Co.,Ltd., Tokyo, Japan, and is marketed under the trade mark APACERAM, which may be registered in some or all of the designated states. The material is available as preformed pieces, such as to th roots, bones for th middle ear and elements for brain surgery and also as a raw material in the form of blocks, which can be worked by sawing, milling and boring and which are of different shapes and porosities, and as a particulate material in the form of granules, i. . particles of regular or

irregular shapes, the sizes of which are of the orders from 0.1 mm to some millimeters. The blocks are used for large implants, preferably after having been properly shaped, and the granules are used for filling bone cavities as well as in combination with said blocks. Thus, since calcium hydroxyapatite is a hard and brittle material as most ceramics are, it is difficult to impart to the blocks the exact shapes needed for the actual implantations, by cutting or otherwise working the blocks, and therefore said granules are used in combination with the shaped block pieces to fill out gaps or spaces existing between the shaped block pieces and the surrounding intact bone tissues.

In most cases the above-mentioned granules or particles are mixed with blood or a physiological saline solution in order to obtain a mass that is easier to apply to the desired site of the bone and to eliminate surface tension phenomena when applying said granules or particules to the bone. A major drawback to this material or technique is, however, that such a mass is not easily properly confined within the bone cavity referred to. Furthermore, when the mass has been applied to the bone, blood that may come from adjacent bleeding portions of the body or any other secreted body fluid will dilute the particulate mass and may even carry away the material from the site of application.

The primary object of the present invention is to overcome last-mentioned drawbacks and to provide an implant material which can be easily and consistently applied to the desired site of action, i.e. where the bone tissue restoration is to be made. More specifically, this means that the new implant material according to the present invention is capable of resisting dilution and any forces tending to carry away the material from the place of application.

These advantages with the present invention will be explained more in detail below as will also other objects of the invention as well as additional advantages therewith.

General disclosure of the invention

The primary object of the invention referred to above is achieved according to a general aspect thereof by providing an implant material composition for r storing bone tissues in a human or animal body, which composition essentially comprises or consists of a solid biocompatible bone tissue substitute material distributed in a bioacceptable mixture of a) a water-based liquid, and b) a monoglyceride or a vegetabilic or animalic oil contain-

ing such a monoglyceride, and optionally c) a triglyceride or a vegetabilic or animalic oil containing such a triglyceride, where said ingredients a), b) and optionally c) are present in the form of an L2 phase or a lamellar liquid crystalline phase and where said ingredients are also present in such proportions that said L2 or said lamellar phase is capable of being transformed into a cubic liquid crystalline phase or a reversed hexagonal liquid crystalline phase when coming into contact with or being contacted with an aqueous liquid.

The biocompatible bone tissue substitute material used according to the present invention generally is the same bone tissue substitute material that has been previously used within this technical field, as was mentioned above when describing the background of the invention. Thus, said material generally is a non-organic material in any particulate form, e.g. granular form. Moreover, it is biocompatible in the general sense of said term.

In other words the general, known principles as to the choices of biocompatible bone tissue substitute materials can be utilized when performing the present invention, but according to a preferable embodiment of the invention said bone tissue substitute material is selected from the group consisting of a mineral, ceramic or metal.

Preferable embodiments of minerals or ceramics are calcium hydroxyapatite, alumina, tricalcium phosphate and calcium aluminate, while the dominating and preferable metal is titanium.

Especially preferable is calcium hydroxyapatite, particularly the non-resorbable type thereof which has the formula $\text{Ca}_{10}(\text{PO}_4)_6(\text{OH})_2$. The main reason therefor is that said compound or mineral is a natural and major constituent of the bones in the body wherein the organic matrix of the bone tissue is received.

The bone tissue substitute material is distributed in a mixture of the above-mentioned ingredients a) and b), optionally also in the presence of c), which mixture forms an L2-phase or a lamellar liquid crystalline phase. In this context the term distributed should be interpreted in a broad sense and generally means spread out in any manner throughout said L2 or lamellar liquid crystalline phase. Expressed in other ways the bone tissue substitute material can be said to be dispersed or slurried in any of the two phases referred to.

A major feature of this aspect of the invention thus is that the ingredients a), b) and optionally c) (when present) are present in such amounts or proportions and conditions that they form an L2-phase or a lamellar liquid crystalline phase. In this context, it should be noted that said expressions L2-phase and lamellar liquid crystalline phase, respectively, are well known to a person skilled in the art and that any more detailed descriptions

thereof should not be needed. Rather, information thereabout can be found in the technical literature, and especially with reference to the nature of the L2-phase reference is made to PCT publication WO 88/00059 and the literature mentioned therein. Thus, although said PCT publication discloses the use of an L2-phase for a completely different purpose the principles and information found therein with reference to L2-phase and also with reference to the lamellar liquid crystalline phase are equally applicable to said phases in connection with the present invention. For instance, said PCT publication discloses that the exact composition of the L2-phase or the lamellar liquid crystalline phase can be found in the prior art, e.g. from a ternary phase diagram. An example of such a phase diagram is also shown in the publication. From such a diagram it can also be gathered that the L2-phase is a liquid single-phase with water-aggregates in a hydrocarbon-continuous medium.

From the above-mentioned it can also be gathered that the mixture forming said L2-phase or lamellar liquid crystalline phase can be a binary system of a) and b) only or alternatively a ternary system where ingredient c) is also present. In both cases, however, the exact compositions to have the desired phases can easily be determined by a person skilled in the art, e.g. by means of a ternary diagram of the type referred to.

However, for the purposes of the present invention it is not sufficient to provide such proportions between the ingredients a), b) and optionally c) that said L2- or lamellar phase is obtained. According to another important feature of the invention the proportions between the ingredients present also have to be selected properly such that the composition obtained is within such specific regions or domains of the L2-phase or lamellar liquid crystalline phase that when the composition is in contact with or is contacted with an aqueous liquid it has to be capable of being transformed into the cubic liquid crystalline phase or the reversed hexagonal liquid crystalline phase. Also these two phases are well known to a person skilled in the art and therefor further information in this respect can be obtained from the prior art. PCT publication No WO88/00059 referred to above gives some information also in this context, but especially with reference to the cubic liquid crystalline phase reference is made to European Patent specification No 126,751. This European Patent specification discloses the use of the cubic liquid crystalline phase for completely different purposes but as was mentioned in connection with the PCT publication said European Patent specification is rather detailed as to the nature of the cubic liquid crystalline phase or the reversed hexagonal liquid crystalline phase, which details are equally ap-

plicable per se to the present invention.

Thus, it can be gathered that the exact composition for which a cubic liquid crystalline phase or a reversed hexagonal liquid crystalline phase is obtained is easily determined by the skilled artisan in a manner known per se, e.g. from a ternary phase diagram. From such a phase diagram one can also easily see where the starting compositions of the L2-phase or the lamellar liquid crystalline phase have to be to obtain the corresponding cubic liquid crystalline phase or reversed hexagonal liquid crystalline phase by mere addition of water or other aqueous liquid.

The basic principle of the present invention and which is utilized for the specific purposes defined herein, which is not in any way disclosed or suggested in any prior art known by us, is that the starting L2-phase or lamellar crystalline phase has the ability to change at constant temperature its state from a liquid condition to a gel-like structure having high viscosity, solely by swelling in the water-based liquid. By mixing the bone tissue substitute material with the mixture forming said L2 or lamellar liquid crystalline phase the bone tissue substitute material will form together with any of said two phases a toothpaste-like mass or similar of a relatively low viscosity, which can easily be applied to a bone cavity or to a bone with an implant body mounted therein or thereupon by smearing the mass onto the surface of said bone or the surface of said bone and said implant, respectively. The viscosity of the mass will then be temporarily increased due to the increased temperature at the application site, but when the mass will come into contact with body fluid, such as blood or the humidity from soft tissue, or any other aqueous liquid it will harden in a very short time, generally in a few seconds, to form a moldable well confined plastic body. This sudden change of the viscosity of the implant material composition is due to the formation of said cubic liquid crystalline phase or said reversed hexagonal liquid crystalline phase when the material referred to is brought into contact with any body fluid or any other liquid present on or supplied to the site of application of the material, said material being a precursor for the formation of the cubic liquid crystalline phase or the reverse hexagonal liquid crystalline phase.

In other words the phase conversion referred to is utilized in a completely new manner and for a completely new purpose, by which the previously known disadvantages within this specific technical field can be reduced or more or less completely eliminated.

In addition to the fact that the mixture of a), b) and optionally c) should of course be bioacceptable, i.e. must not cause any significant side effects in contact with living cells or organisms, it

could be added that generally the viscosity considerations as to the different phases refer to temperatures at or around normal body temperatures as the composition is intended for use in contact with the body. This generally means that the viscosity of the starting phase as well as that of the transformed phase should be selected, preferably by choice of materials, so as to be proper, i.e. liquid, below a temperature of about 40°C for the intended purpose. More specifically this means that preferable embodiments of the three ingredients a), b) and c) are as follows.

The water-based liquid a) is any liquid wherein water is the major or dominating part. This means that pure water or an isotonic salt solution is preferably utilized, but if advisable for any reasons any aqueous body fluid or other aqueous liquid may be used.

The monoglyceride b), which can be used in the form of one single monoglyceride or as a mixture thereof, generally is a monoglyceride of an unsaturated fatty acid. Preferably said unsaturated fatty acid is an unsaturated C₁₆-C₂₂-fatty acid. An especially preferable embodiment thereof is a C₁₈-fatty acid, particularly monoolein. Said monoolein, which is the glyceride of oleic acid, is preferably utilized in the form of 1-monoolein or a mixture of 1-monoolein and 2-monoolein, said mixture preferably being an equilibrium mixture thereof.

However, often it is not necessary to utilize the monoglyceride per se. Instead any vegetalistic or animalistic product containing the same, such as a vegetalistic or animalistic oil containing the desired monoglyceride, can be used, which may even be a preferred embodiment.

The triglyceride when used as ingredient c) generally is a triglyceride of an unsaturated fatty acid. As in connection with the monoglyceride said triglyceride is preferably a triglyceride of an unsaturated C₁₆-C₂₂-fatty acid, more preferably a C₁₈-fatty acid. Nor the triglyceride has to be utilized as such but rather it may be preferable to use any nature product containing the same, such as any vegetalistic or animalistic oil containing the desired triglyceride. A preferable example of such a nature product is soybean oil. Furthermore, mixtures of triglycerides may be utilized if desired.

Although the specific ratios between the ingredients of the mixture of a), b) and c) (if present) are individually determined for each specific case, e.g. from a ternary phase diagram, preferably embodiments with reference to such compositions, mainly for viscosity reasons, are the following.

A preferable weight ratio of monoglyceride b) to water-based liquid a) is within the range of about 97:3 - 85:15, a range of about 97:3 - 95:5 being especially preferable in many cases.

Especially in a case where a ternary system is

used preferable weight percentages of the ingredients, based on the total weight of a) + b) + c), are about 2-15 percent of the waterbased liquid a), about 80-98 percent of the monoglyceride b) and about 0-12 percent of the triglyceride c). A preferable range of a) is within 2-8%, especially 3-5%, while a preferable range of b) is 85-98% or 80-90%. If present, c) is preferably used within the range of 2-12%. A specific, interesting weight ratio within the above-mentioned range is about 5:85:10, i.e. expressed as a):(b):(c).

Generally, although the bone tissue substitute material may be a minor volume constituent the volume ratio of bone tissue substitute material to the total of a) plus b) plus c) (when present) is within the range of 1:1 - 5:1, a range of about 1:1 - 3:1 being especially preferable for many applications. The optimum ratio, especially in the case of calcium hydroxyapatite, is around 3:1 by volume.

The invention also relates to a method of preparing the above-identified implant material composition. Said method essentially comprises forming the L2 or lamellar liquid crystalline phase of said ingredients a), b) and optionally c) and then distributing the bone tissue substitute material therein.

If the monoglyceride or triglyceride is not in the liquid state at the temperature where said L2 or lamellar liquid crystalline phase is formed any one thereof is generally melted before the water-based liquid is added thereto.

As concerns the conditions for forming an L2 or lamellar liquid crystalline phase reference is made to the prior art, and with reference to the distribution of the bone tissue substitute material therein reference is made to the specification above. Thus, any suitable method of distributing a solid material in a phase of the type referred to can be utilized.

The preferable embodiments described above in connection with the implant material composition are equally applicable to the method according to the invention of preparing said composition.

Moreover, the present invention provides a method of restoring lost bone tissue in a bone of a human or animal body, which comprises applying the implant material composition as defined above to the surface of any bone or bone cavity where lost bone tissue is to be restored and allowing said composition to come into contact and/or contacting the same with an aqueous liquid in such an amount that said composition will be transformed or converted into the corresponding cubic liquid crystalline phase or the corresponding reversed hexagonal liquid crystalline phase.

The starting L2 or lamellar liquid crystalline phase is preferably chosen so as to have a viscosity which enables the use of a conventional one-

way syringe, the low viscosity implant material being received by the syring and being ejected th r from to the region of the bone where th mass is to be applied.

Irrespective of the method of application, however, the applied composition changes its phase to a cubic liquid phase or a reversed hexagonal liquid phase in contact with the aqueous liquid as defined above, a well confined plastic mass of high viscosity being formed at the site of application.

After said phase conversion the applied material may be given the final form at the application site by a plasti working of the materiai. The implant material can also be fixed by being covered with surrounding soft tissue which is closed by suturing.

Although the method just referred to has been described and will be more specifically described below as a method of shaping the implant product at the ultimate site of application, it is also within the scope of the invention to make a preshaping of the product outside the body in any suitable mold by bringing the implant material composition into contact with the water-based liquid and then making the final shaping and fixing in the desired bone cavity.

The preferable embodiments described above in connection with the implant material composition are equally applicable to the method of restoring lost bone tissue just described.

The invention also relates to the composition as defined above, also as to all preferable embodiments thereof, for use as an implant material composition for restoring bone tissue in a human or animal body.

Furthermore, the invention relates to the use of the abovementioned composition for the manufacture of a product or preparation to be used as an implant material for restoring bone tissue in a human or animal body. All preferable embodiments described above in connection with the implant material composition are equally applicable to this aspect of the invention.

Finally, the invention also provides the restored implant bone tissue product per se, i.e. the product that is obtainable or obtained by contact between the implant material composition as defined above with an aqueous liquid, said product being in the state of a cubic liquid crystalline phase or a reversed hexagonal liquid crystalline phase. All preferable embodiments disclosed above are applica ble also to this aspect of the invention.

As was mentioned above the major advantage of the present invention is that the handling of the bone substitute material will be considerably facilitated and that particles thereof are prevented from escaping from the application site. If this would happen the particles could cause irritation or com-

plication at other places of the body.

Another advantage in connection with the invention is that the composition can be sterilized and can be stored in closed packages without any changes of properties.

Other advantages could be gathered from the present specification or should be obvious to a person skilled in the art.

The drawings

The invention will now be described with reference to the accompanying drawings, which show non-limiting embodiments of the invention only and wherein

FIG. 1 is a phase diagram of a monoolein-water mixture;

FIG. 2 is a diagrammatic plan view of a skull portion with an implant product therein; and

FIG. 3 shows a schematic phase diagram for the system of sunflower oil monoglyceride/soybean oil/water at 40°C and 90°C.

An ideal monoglyceride for use in connection with the present invention is oleic acid, inter alia because it is not easily oxidized which might cause risks of the formation of toxic substances. Reference is made to the diagram shown in figure 1, which is a phase diagram for a mixture of monoolein and water indicating the relationship between temperature and water content related to the existence of the phase wherein the monoolein-water mixture is liquid and the phase wherein the monoolein-water mixture has a gel-like structure with high viscosity. If the water phase contains salts of physiological concentrations or proteins from the blood or lymph system the diagram will not be changed.

Thus, starting from monoolein having a water content of about 4% (weight by weight) the phase is liquid in the temperature range from about 20 to 40°C, i.e. below the body temperature (about 36°C). This phase is indicated as L₂ because the water molecules thereof form a reversed micellar structure. After swelling in contact with water or any other aqueous liquid, such as blood or the humidity of soft tissue, the viscous phase D (D stands for diamond glitter which is the water canal structure of the phase) will be obtained, which is the cubic liquid crystalline phase. The other phases shown in the figure are: L_a=lamellar liquid crystalline phase; H_{II}=reversed hexagonal liquid crystalline phase; and G=gyroid, which is also a cubic liquid crystalline phase.

An implant material of the D phase of monoolein in soft tissue and in bone tissue has been found to be perfectly biocompatible therewith and to cause no changes of inflammatory characters. Probably this is due to the fact that monoolein is

present in the body and will be exchanged with esterases (lipases) in the normal lipid metabolism. Another favorable factor probably is that the cubic structure is identical with the lipid structure of biological membranes, i.e. a bimolecular layer with the polar group facing outwardly towards the water medium.

In order to obtain the favorable liquid L₂ phase at about room temperature the water content of the monoolein-water mixture should preferably be within the range of from about 3.5 to 4% (weight by weight). Thus, such a liquid L₂ phase has been found to be especially preferable as it imparts ideal consistency conditions to the implant material. However, higher water contents are also possible for this specific case, as then the lamellar liquid crystal phase will be formed, which phase is also of such a viscosity that it is useful in accordance with the present invention.

In figure 2 there is shown a plate 10 obtained from a block of calcium hydroxyapatite which plate is located and suitably fixed in an opening 11 of a skull portion 12. The implant material composition can be applied to the plate and the surrounding region of the scull indicated by hatching at 13 by dispensing the low viscosity implant material composition from a syringe wherein it has been stored, and the composition is then smeared out at least in the region 13.

When the composition is contacted with the scull the viscosity thereof may decrease due to a temperature rise but when the composition comes into contact with any body fluid, such as blood, the viscosity thereof will increase in a few seconds so as to form a well confined mass of high viscosity which can still be plastically worked at the site of application so as to impart to the material the desired shape and to provide a smooth and tight transition between the plate and the surrounding bone of the scull. Thus, by means of the implant material applied inaccuracies are equalized between the plate 10 and the edges of the opening 11 due to difficulties to accurately work the hard and brittle calcium hydroxyapatite blocks to the exact form of the opening.

The applied implant material may be fixed in the intended position by covering the scull and the implant region by means of surrounding soft tissue which is then closed by suturing.

Fig. 3 shows a phase diagram for one useful composition according to the invention, i.e. sunflower oil monoglyceride, soy bean oil triglyceride/water at 40°C and 90°C.

The two-phase regions and three-phase triangles are marked at 40°C only. The meanings of the symbols are: L₂, isotropic "oily" solutions; C, cubic liquid crystalline phase; D, lamellar liquid crystalline phase; and F, reversed hexagonal liquid

crystalline phase. In other words, the starting implant material composition according to the invention is within that part of the L2- or D-phase where addition of water or aqueous liquid will give a composition (and a phase conversion) within any of the C- or F-phases, respectively.

Examples

The invention will also be more specifically described by means of the following non-limiting examples.

EXAMPLE 1

Monolein is heated to a temperature just above the melting point thereof (36°C) and not above 40°C . When the monolein is completely melted a physiological saline solution of the same temperature (just below 40°C) is added so as to obtain a weight ratio of monolein/water of 96.2:3.8.

The resulting L2 phase is allowed to cool to room temperature and then granules of calcium hydroxyapatite, APACERAM®, are added, with stirring, said addition being made to a volume ratio of calcium hydroxyapatite:L2 solution of 3:1

The implant material composition thus obtained has a toothpaste-like consistency and can be stored in closed packages, e.g. a one-way syringe, at a temperature ranging from about 0°C to 40°C without any changes of properties. When the composition is to be used a temperature within the range of from 20°C to 35°C should be imparted thereto. In this context it should be noted that a rise of temperature will mean a lowering of the viscosity.

When applied to a bone cavity the composition sucks up body fluid and/or blood into the structure and a dramatic increase of viscosity is obtained due to the conversion of the L2 phase into a cubic liquid crystalline phase which ultimately gets saturated. The mixture obtained is stiff but still moldable.

EXAMPLE 2

As in example 1 monolein is heated just over the melting point thereof (36°C). Soybean oil is added to the melted monolein and then a physiological saline solution is added thereto, the weight ratio of monolein/soybean oil/water being 85:10:5.

After cooling of the resulting L2 phase to room temperature granules of calcium hydroxyapatite (APACERAM®) are added thereto as in example 1 to a ratio of calcium hydroxyapatite/L2-solution of 3:1 by volume. The composition thus obtained has a lower viscosity than the composition obtained according to example 1, and the viscosity thereof

will be further reduced if adding more soybean oil.

The composition behaves in a manner similar to that of the composition described in example 1 when applied to bone in a human or animal body. That is, a phase conversion to the cubic phase is obtained.

EXAMPLE 3

As in the previous Examples monolein is heated just above the melting point thereof (36°C). A physiological saline solution is added thereto, the weight ratio of monolein/water being 86:14.

After cooling the L2 phase thus obtained to room temperature granules of the same calcium hydroxyapatite as in Example 1 and 2 are added to a volume ratio of calcium hydroxyapatite: L2 phase of 2:1. The composition obtained has a lower viscosity than the one prepared in Example 1 but higher than that prepared in Example 2.

When applied to a bone cavity the composition sucks up body fluid and/or blood and the ultimate water content thereof increases to about 39% of the total weight when the cubic phase is saturated. During the phase conversion the viscosity increases dramatically to a stiff but still formable mixture. The time for said phase conversion depends on the body volume of the mixture, but generally it is of the order of 10-60 seconds for a volume of 1 cm^3 .

Claims

35. 1. An implant material composition for restoring bone tissue in a human or animal body, characterized in that it comprises a solid, preferably particulate, biocompatible bone tissue substitute material distributed in a bioacceptable mixture of a) a water-based liquid and b) a monoglyceride or a vegetabilic or animalic oil containing a monoglyceride, and optionally c) a triglyceride or a vegetabilic or animalic oil containing a triglyceride, a), b) and optionally c) forming an L2-phase or a lamellar liquid crystalline phase and being present in such proportions that said L2 or lamellar phase is capable of being transformed into a cubic liquid crystalline phase or a reversed hexagonal liquid crystalline phase when contacted with an aqueous liquid.
40. 2. A composition according to claim 1, characterized in that the monoglyceride defined in b) is a monoglyceride of an unsaturated fatty acid.
45. 3. A composition according to any one of the preceding claims, characterized in that the triglyceride defined in c) is a triglyceride of an unsaturated fatty acid.
50. 4. A composition according to claim 2 or 3, char-

acterized in that said unsaturated fatty acid is an unsaturated C₁₆-C₂₂-fatty acid.

5. A composition according to claim 4, characterized in that said C₁₆-C₂₂-fatty acid is a C₁₈-fatty acid.

6. A composition according to claim 5, characterized in that the monoglyceride is monoolein, preferably 1-monoolein or a mixture of 1-monoolein and 2-monoolein.

7. A composition according to claim 5, characterized in that the triglyceride is soy bean oil.

8. A composition according to any one of the preceding claims, characterized in that the weight ratio of monoglyceride b) to water-based liquid a) is within the range of about 97:3 - 85:15.

9. A composition to any one of claims 1-7, characterized in that the weight percentages of the ingredients a), b) and c), based on the total weight of a) + b) + c), are about 2-15%, preferably 3-5%, of the water-based liquid a), about 80-98%, preferably 85-98%, of the monoglyceride b) and about 0-12%, preferably 2-12%, of the triglyceride c).

10. A composition according to any one of the preceding claims, characterized in that said bone tissue substitute material is selected from the group consisting of a mineral or ceramic, such as calcium hydroxyapatite, alumina, tricalcium phosphate and calcium aluminate, and a metal, such as titanium.

11. A composition according to claim 10, characterized in that said bone tissue substitute material is selected from the group consisting of calcium hydroxyapatite, alumina, tricalcium phosphate and calcium aluminate.

12. A composition according to claim 11, characterized in that said bone tissue substitute material comprises calcium hydroxy apatite.

13. A composition according to any of the preceding claims, characterized in that the volume ratio of bone tissue substitute material to a) plus b) and optionally c) is within the range of 1:1 - 5:1.

14. A method of preparing an implant material composition as defined in any one of claims 1-13, characterized by forming said L2 or a lamellar liquid crystalline phase of the ingredients a), b) and optionally c) and distributing said bone tissue substitute material therein.

15. A method according to claim 14, characterized by melting b) and/or c) where necessary before adding a) thereto to form said L2 or lamellar liquid crystalline phase.

16. A method of restoring lost bone tissue in a bone of a human or animal body, characterized by applying an implant material composition as defined in any one of claims 1-13 to the surface of any bone or bone cavity where lost bone tissue is to be restored and allowing said composition to come into contact and/or contacting the same with

an aqueous liquid in such an amount that said composition will be transformed into a cubic liquid crystalline phase or a reverse hexagonal liquid crystalline phase forming a plastic mass that is well confined within said bone cavity.

5 17. A method according to claim 16, characterized in that said implant material composition is supplied to the site of application by means of a syringe.

10 18. A restored implant bone tissue product obtainable by contact between the implant material composition as defined in any of claims 1-13 and an aqueous liquid, said product being in the state of a cubic liquid crystalline phase or a reversed hexagonal liquid crystalline phase.

15 19. A composition as defined in any one of claims 1-13 for use as an implant material composition for restoring bone tissue in a human or animal body.

20 20. Use of a composition as defined in any one of claims 1-13 for the manufacture of a product to be used as an implant material for restoring bone tissue in a human or animal body.

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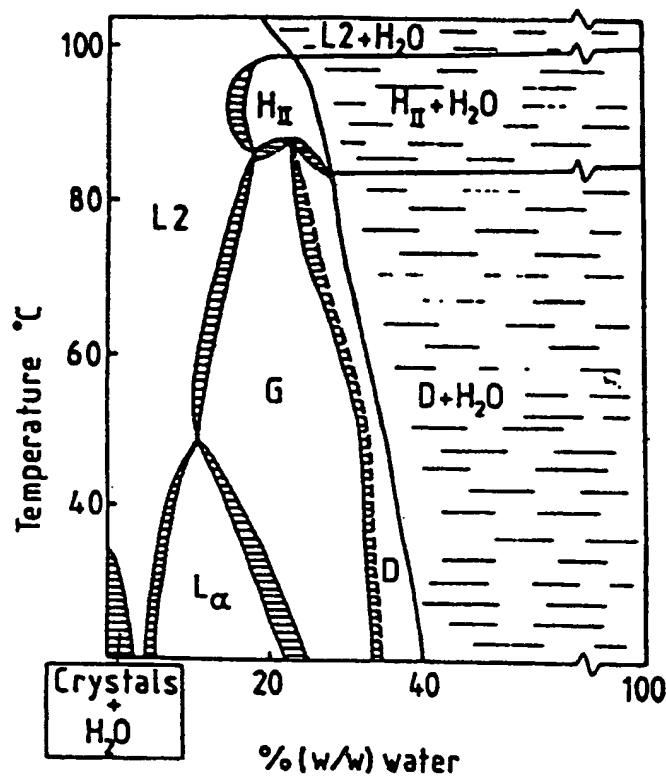


Fig. 1

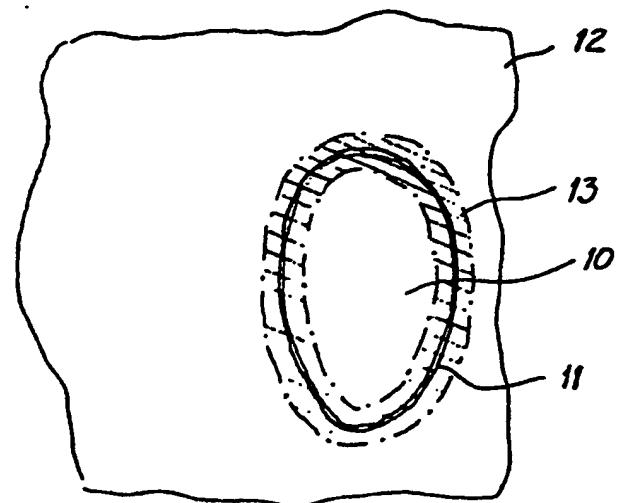


Fig. 2

